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APPLICATION OF NANOPARTICLES IN MODERN DRUG DELIVERY AND TECHNOLOGY

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ABSTRACT

Many novel nanocarriers have been developed as a result of recent research on modified nanoparticles in drug delivery systems (DDSs). Both conventional and contemporary drug delivery techniques are examined in this review. Nanocarriers have garnered a lot of interest because of the shortcomings of traditional DDSs. Polymeric nanoparticles, mesoporous nanoparticles, carbon nanotubes, dendrimers, liposomes, metallic nanoparticles, nanomedicine, and tailored nanomaterials—all of which are intended to deliver medications to certain locations within the body—are among them. Rapid advancements in nanomedicine are being used to treat a variety of illnesses, including lung, breast, brain, and cardiovascular ailments. Improved medication bioavailability, quicker absorption, regulated release, inhibition of drug aggregation, and increased bloodstream solubility are just a few benefits of these systems. By maximising the therapeutic potential of active pharmaceutical components encased in nanoparticles, nanomedicine represents a revolutionary breakthrough in drug delivery. Important information about manufactured nanoparticles and their uses in targeted medication delivery for a range of illnesses is compiled in this overview. The majority of these nanocarriers have been tested both in vivo and in vitro. Future developments in nanomedicine are anticipated to greatly improve human health by increasing the efficacy of drug delivery systems.

Keywords: Drug Delivery, Nanomedicine, Therapeutics, Nanoparticles, Personalized Medicine.

INTRODUCTION

Many different diseases have long been treated with drug delivery systems (DDSs). To have therapeutic effects, all pharmaceuticals rely on pharmacologically active substances, or drugs [1]. Certain medications are given as inactive precursors, which the body must metabolise before they become active [2]. The way these medications are administered has a big impact on how well they work. Drugs were typically given orally, nasally, via inhalation, through mucosal routes, or by injection in conventional drug delivery systems (CDDSs) [3]. Nevertheless, these techniques frequently led to inadequate absorption, haphazard distribution, inadvertent harm to healthy tissues, early removal from the body, and extended treatment durations [4].

Enzymatic breakdown, pH fluctuations, mucosal barriers, imprecise targeting, and the quick release of medications that could raise systemic toxicity were some of the reasons that limited their efficacy [5]. The deliberate engineering and manipulation of particulate matter into a physical state of 1 nm to 100 nm that may be rearranged or reassembled into nano-systems with enhanced functionality is known as nanotechnology [6]. For example, Ireland has been at the forefront of scientific research in the past ten years due to the development of nanotechnology and its applications [2]. Depending on their size, nanoparticles—the final product of technological alteration of matter—are a few degrees bigger than an

atom as a result of the molecular processing of matter. Compared to traditional substances, they are highly adaptable and can be adjusted to obtain a specific characteristic or targeted properties like high surface area because they have enhanced characteristics like auto-reactive stability and self-reassembly [3, 4]. Significant progress in the discipline was sparked by physicist Richard Feynman's 1959 speech "There's Plenty of Room at the Bottom," which introduced the idea of nanotechnology [15]. At the nexus of several scientific fields, including physics, chemistry, biology, engineering, information technology, electronics, and materials science, nanotechnology entails the study and manipulation of incredibly small structures [16]. Structures at the nanoscale usually fall between 1 to 100 nm [17]. Nanoparticles have a variety of uses in engineering, drug delivery, nanomedicine, environmental remediation, catalysis, and the treatment of diseases like melanoma, cardiovascular diseases (CVD), skin disorders, liver diseases, and more because of their submicroscopic size [18]. Drug efficiency and bioavailability could be increased by combining nanotechnology with medicine [19]. Since the late 1970s, the relationship between nanoparticles and biomedicine has been acknowledged, resulting in over 10,000 publications mentioning nanomedicine, of which about thirty had appeared by 2005 [20]. Over 1,000 publications on nanomedicine have been published in the Web of Science by 2015, the majority of which concentrated on the biological uses of nanoparticles [21]. Advanced forms of nanocarriers include dendrimers, liposomes, peptide-based nanoparticles, carbon nanotubes, quantum dots, polymer-based nanoparticles, inorganic vectors, lipid-based nanoparticles, hybrid nanoparticles, and metallic nanoparticles [22]. These nanocarriers are increasingly used in drug delivery, microfluidics, biosensors, microarrays, and tissue engineering for targeted disease treatment [23–25]. Nanoparticles can selectively target and destroy cancer cells, offering promising cancer therapies [26]. For example, in 2015, the FDA approved clinical trials for Onivyde, a nanomedicine used in cancer treatment [27]. Nanocarriers possess specific physicochemical properties that enhance drug solubility, stability, targeting, degradation control, clearance, theragnostic, and combination therapies [28]. Protein-based nanomedicines have also been explored, in which various protein subunits assemble to deliver drugs directly to tumors [29]. These protein-based nanocarriers include nanoparticles, hydrogels, films, microspheres, nanorods, and Mini pellets, constructed from proteins such as ferritin cages, small heat shock proteins (sHsp), plant-derived viral capsids, albumin, soy and whey proteins, collagen, and gelatine [30,31]. Nanomedicine represents a new era in drug delivery, enabling the design of targeted structures that carry multifunctional payloads with improved pharmacokinetics, specificity, efficacy, and safety (Figure 2) [32,33]. Failures in traditional chemotherapy have increased the risk of disease recurrence, further complicating the treatment of life-threatening conditions [34].

History

Petros and his associate examined nanotechnology advancements that date back to the middle of the 20th century. The first conjugation of polymers with drugs occurred in 1955 [35], the first controlled-release polymer device was introduced in 1964, Bangham discovered liposomes in 1965, albumin-based nanoparticles appeared in 1972, liposome-based drugs were developed in 1973, the first micelle formulation was developed and approved in 1983, the FDA approved the first controlled-release formulation in 1989, and the first polyethylene glycol (PEG)–protein conjugate hit the market in 1990 [36]. As summarised, subsequent research has yielded extremely promising results for the treatment of numerous disorders.

Over the past three decades, various types of nanoparticles (NPs) have been developed as drug delivery systems, each with unique approaches, disease targets, applications, characterization methods, and reported studies. In 1991, poly-alkyl-cyanoacrylate nanoparticles were introduced as carriers for site-specific drug delivery in cancer therapy, particularly for chemotherapy and intracellular antibiotherapy, characterized by scanning electron microscopy [37,38]. In 1992, calcium hydroxyapatite ceramic (CHC) was used to load gentamicin in porous blocks for treating chronic osteomyelitis in animal models, retaining bactericidal activity despite the absence of *in vivo* experiments [39,40]. By 1993, micro- and nanoparticles were explored for oral immunization, with mechanisms such as self-diffusion and pulsed drug release, evaluated through *in vitro* experiments [41,42]. In 1994, acrylic acid copolymer nanoparticles were applied to enhance opsonin targeting and the reticuloendothelial system, analysed by small-angle X-ray scattering [43,44].

In 1995, poly-alkyl-cyanoacrylate (PECA) nanoparticles entrapping ofloxacin and perfloxacin improved antimicrobial activity for bacterial infections, characterized by freeze–fracture electron microscopy [45,46]. Protein and peptide-based nanoparticles were applied in 1996 for Alzheimer's disease, delivering monoclonal antibodies and recombinant proteins across the blood–brain barrier (BBB) via chimeric peptide approaches, although physiological characterization was not performed [47,48]. In 1997, nanoparticles were utilized in intra-arterial catheter-based delivery for restenosis, showing high biocompatibility without injury [49,50]. By 1998, deblock copolymer nanoparticles in micelles and nanospheres were developed to sustain drug release, enhance solubility, and improve circulation time, though no *in vivo* characterization was reported [51,52].

In 1999, chitosan nanoparticles enhanced insulin absorption through the nasal cavity for diabetes management, characterized by zeta potential and photon correlation spectroscopy [53,54]. In 2000, liposomes combined with hyperthermia improved targeted drug delivery for ovarian carcinoma, demonstrating effective results in experiments

[55,56]. PEGylated poly-cyano-acrylate nanoparticles introduced in 2001 extended drug circulation for prion diseases, with higher brain and spleen uptake in scrapie-infected models [57,58]. Transferrin-mediated receptor endocytosis in 2002 enabled targeted drug and gene delivery to cancer and brain diseases by exploiting transferrin receptor pathways, though characterization was limited [59,60].

By 2003, L-nanoparticles demonstrated targeted delivery to hepatocytes for Hepatitis B, hepatocellular carcinoma, and haemophilia, showing specificity in xenograft mouse models [61,62]. Colloidal gold nanoparticles in 2004 served as vectors for tumor necrosis factor delivery in carcinoma models, analysed by TEM and light scattering [63,64]. In 2005, folate-conjugated liposomes carrying chemotherapeutics and DNA enabled targeted gene transfer in nasopharyngeal and prostate cancer cells [65,66], while folate-conjugated starch nanoparticles in 2006 targeted liver cancer with doxorubicin, reducing toxicity and enhancing targeting [67,68]. Gold nanoparticles in 2007 facilitated drug and gene delivery in carcinoma cells with reduced toxicity and high transfection efficiency [69,70], and PEGylated gold nanoparticles in 2008 improved in vivo photodynamic cancer therapy with targeted tumor delivery [71,72].

Alginate/chitosan nanoparticles developed in 2009 optimized size and loading parameters for drug delivery via zeta potential and FTIR analysis [73,74], while mesoporous silica nanoparticles in 2010 achieved targeted methotrexate delivery to tumor cells with high cell specificity and low cytotoxicity [75,76]. Nano-diamonds in 2011 delivered small interfering RNA into cancer cells efficiently without structural damage, as confirmed by FTIR and zeta potential analysis [77,78]. Silver nanoparticles emerged in 2012–2014 as vectors for antimicrobial and photo-activated gene silencing, synthesized through green methods and characterized by UV-visible spectroscopy, TEM, and FTIR, showing applications in malaria, dengue, and vector control [79–84].

Polyamidoamine nanoparticles in 2015 served as carriers for anti-malarial drugs, improving solubility, circulation time, and targeting with reduced toxicity [85,86]. Solid lipid nanoparticles in 2016 enabled delivery of photosensitizers and flavonoid derivatives for colon cancer treatment, evaluated by confocal microscopy and DLS [87,88]. In 2017, filamentous bacteriophage-based nanoparticles facilitated targeted drug and gene delivery for bacterial and viral diseases, representing a unique virus-based system [89,90]. Mesoporous silica nanoparticles in 2018 were engineered for siRNA delivery through electrostatic absorption, offering a cost-effective non-viral vector solution [91,92]. Chitosan nanoparticles in 2019 proved versatile for ocular, nasal, pulmonary, buccal, and mucosal drug delivery, including vaccine delivery and cancer treatment [93,94].

In 2020, folic-acid-functionalized mesoporous silica nanoparticles were developed as pH-sensitive systems for targeted cancer therapy, offering prolonged drug release characterized by XRD, TEM, HNMR, SEM, and TGA [95,96]. In 2021, novel silver nanoparticles were applied for mRNA and DNA delivery to stimulate immune responses against SARS-CoV-2, while lipid-based, metal, and resveratrol–zinc nanoparticles demonstrated roles in COVID-19 prevention and therapy, including vaccines and immune sensors [97–100]. In 2022, iridium oxide and chitosan nanoparticles were synthesized as biocompatible nanoproboscopes for in vivo cancer therapy and neural regeneration, combining photothermal and drug delivery capabilities without immunogenicity [101,102].

Recent Approaches in Drug Delivery Systems for Various Diseases

Brain Drug Delivery Systems and Their Types

The blood–brain barrier (BBB) is impaired in many clinical situations, including as strokes, seizures, multiple sclerosis, AIDS, diabetes, glioma, Alzheimer's disease, and Parkinson's disease [103]. Under such diseased conditions, structural remodelling of protein complexes at endothelial junctions is largely responsible for this breakdown [104]. By preventing macromolecules and tiny compounds from entering the bloodstream, the blood-brain barrier (BBB) normally maintains brain homeostasis [105]. Nevertheless, if a medication does get across the blood-brain barrier, it frequently leads to decreased bioavailability and buildup inside brain tissue, which restricts the efficacy of treating brain illnesses [106].

To overcome this challenge, advanced drug delivery systems (DDS) such as cell membrane-based DDS, virus-mediated DDS, or exosome-based DDS are engineered to possess BBB penetration ability, lesion targeting, and safety [107]. Among these, nanocarrier-assisted intranasal delivery has become a prominent method for brain therapy [108]. At an advanced stage, drugs with poor brain distribution can be loaded into nanocarriers that interact with endothelial microvessel cells of the BBB and nasal mucosa, increasing drug residence time and enabling direct nose-to-brain delivery via olfactory nerve pathways [109]. This process improves drug absorption into brain parenchyma through a secondary nose-to-blood-to-brain pathway [110].

Current strategies for brain drug delivery include viral vectors, nanoparticles, exosomes, BBB permeability enhancers, active transporter-based delivery across the BBB, alternative administration routes, nanoparticles specifically designed for brain delivery, and advanced imaging/diagnostic systems under pathological conditions [111].

Role of Nanocarriers in Alzheimer's Disease

Alzheimer's disease (AD) is one of the fastest-growing neurodegenerative disorders in the elderly, characterized by memory loss, diminished verbal abilities, and impaired spatial reasoning [112]. A hallmark of AD is the accumulation of amyloid β ($A\beta$) plaques, which contribute to cognitive dysfunction [113]. Nanotechnology-based drug delivery approaches have proven useful in treating such conditions [114]. In AD, delivery systems such as polymeric nanoparticles, liposomes, solid lipid nanoparticles, nanoemulsions, microemulsions, and liquid crystals are employed.

Polymeric Nanoparticles:

1. Tacrine-loaded polymeric nanoparticles administered intravenously enhance brain concentration of the drug while reducing the total dose required [115].
2. Rivastigmine-loaded polymeric nanoparticles administered intravenously improve learning and memory [116].

SLNPs:

SLNPs improve drug retention in the brain and enhance BBB permeability [117]. Examples include: Piperine-loaded SLNPs administered intraperitoneally reduce plaques and masses while enhancing acetylcholinesterase (AChE) activity [118].

1. Huperzine A-loaded SLNPs improve cognitive functions without significant irritation in rat skin studies [119].
Coating SLNPs with surfactants like polysorbate improves bioavailability [120,121]. Examples include:
 1. Clozapine in a Dynasan 116 lipid matrix coated with Poloxamer 188 and Epikuron 200 for safe brain delivery [122,123].
 2. Vitamin A in Glyceryl behenate lipid matrix coated with hydroxypropyl distarch [124,125].
 3. Diminazine in stearic acid matrix coated with polysorbate 80 for targeted delivery [126,127].
 4. Doxorubicin in stearic acid SLNPs coated with Taurodeoxycholate for effective drug delivery without loss of potency [128,129].

Liposomes:

Liposomes are promising carriers for brain-targeted drug delivery due to their capacity to encapsulate large amounts of drug and their ability to be functionalized with ligands [130–132]. Examples:

1. Curcumin–PEG-loaded liposomes showed high binding affinity to senile plaques and inhibited $A\beta$ aggregation in ex vivo studies, with BBB uptake demonstrated in rats [133].
2. Folic acid-loaded liposomes administered intranasally enhanced drug absorption through the nasal cavity [134].

Nano emulsions:

Beta-Asarone loaded in nano emulsions and administered intranasally improved bioavailability [130].

Microemulsions:

Tacrine-loaded microemulsions administered intranasally enhanced memory performance [135].

Liquid Crystals:

T. divaricate-loaded liquid crystals delivered trans dermally prolonged drug retention and improved skin penetration [136].

Role of Nanocarriers in Parkinson's Disease (PD)

Parkinson's disease (PD) is the second most common neurodegenerative disorder and presents significant challenges in effective drug delivery and diagnosis [137]. Levodopa, the conventional treatment, suffers from poor bioavailability and limited brain penetration [138]. Nanotechnology offers promising strategies to overcome these limitations, employing metal nanoparticles, quantum dots, cerium oxide nanoparticles, organic nanoparticles, liposomes, and gene therapy to enable drugs to cross the BBB [139,140].

For example, Bhatta Misra et al. demonstrated that retigabine-loaded chitosan nanoparticles delivered via the intranasal route in a rat PD model achieved better brain delivery, as confirmed by pharmacokinetic studies [125].

Ropinirole (RP):

RP-loaded solid lipid nanoparticles (RP-SLNPs) and nanostructured lipid carriers (RP-NLCs) in hydrogel formulations improved oral and topical drug delivery [141]. These formulations proved to be effective carriers for delivering RP to the brain for PD treatment [142,143].

Mechanism of Nanoparticles in Brain Drug Delivery (Across BBB)

Nanoparticles are typically administered through intranasal, intraventricular, or intraparenchymal routes, enabling them to cross the BBB due to their small size. Upon reaching the BBB, nanoparticles use mechanisms such as receptor-mediated transport, active transport, or passive diffusion to enter the brain. Their small size facilitates passive diffusion across endothelial cells, and their surface properties allow interaction with brain receptors and ligands to enhance targeted delivery (Figure 3) [144].

Tacrine-loaded polymeric nanoparticles (NPs)

Advantages:

1. Prolonged retention in the brain
2. High biocompatibility
3. Low cost of production
4. Controlled drug release
5. Ability for targeted delivery via ligand conjugation

Disadvantages:

1. Slow biodegradation
2. Potential uncertainty in toxicity[145]

Rivastigmine-loaded polymeric NPs

Advantages:

6. Increased drug concentration in the brain
7. Avoidance of phagocytosis by the reticuloendothelial system (RES)

Disadvantages:

1. Possible increase in oxidative stress
2. Potential toxicity concerns[146]
2. **Piperine-loaded solid lipid nanoparticles (SLNPs)**

Advantages:

1. Extensively studied for drug delivery
2. Reduced side effects compared to free drugs
3. Enhanced therapeutic efficacy
4. Improved drug solubility

Disadvantages:

1. Low drug-loading capacity
2. Rapid clearance by the reticuloendothelial system[147]
3. **Folic-acid-loaded liposomes**

Advantages:

1. Excellent biocompatibility and biodegradability
2. High stability and bioavailability
3. Active surface targeting possible

Disadvantages:

1. Difficulty in lipid binding
2. Lower stability and reduced drug carriage efficiency [148]

Role of Nanocarriers in Major Cancers

Brain Cancer

One of the hardest diseases to successfully treat is brain cancer [150]. The blood–brain barrier (BBB), which restricts the passage of therapeutic medicines to the brain, is a major cause of the problem [151]. The brain's microvascular endothelium forms the blood-brain barrier (BBB), which is a selective barrier that keeps blood and neural tissues apart [152]. By keeping dangerous poisons, xenobiotics, and other metabolic chemicals out of the brain, this barrier is essential for brain protection [153]. Glioma and glioblastoma are two common types of brain cancer that are extremely aggressive and deadly [154].

These cancers occur at a rate of approximately 5.26 cases per 100,000 individuals, equating to around 17,000 new diagnoses annually. Standard treatments typically involve surgery, radiation, and chemotherapy, often combined with temozolomide (TMZ) [155]. Nanoparticles offer significant promise in brain cancer therapy due to their nanoscale size, ability to specifically target tissues, and capability to cross

In recent years, a variety of nanoparticles (NPs) have been explored treatment due to their ability to improve drug delivery across the blood–brain barrier for brain cancer and enhance therapeutic outcomes. Gold nanoparticles (DOX-SL-GG AuNPs) loaded with doxorubicin have shown increased cytotoxic activity through endocytosis in glioma and glioma stem cell lines, particularly in LN-229 and HNGC-2 cells [157,158]. Albumin-bound nanoparticles carrying lapatinib have been effective in constraining migration, invasion, and adhesion of high brain-metastatic cells in murine models [159,160]. Similarly, lipoprotein-like nanoparticles loaded with lapatinib significantly inhibited tumor growth in U87 glioma xenografts in vivo [161,162]. Gold–iron oxide nanocomposites conjugated with curcumin–lipoic acid exhibited greater cytotoxicity against U87MG brain cancer cells compared to normal astrocytes [163,164]. Tocopherol polyethylene glycol chitosan nanoparticles, loaded with docetaxel, enhanced cellular uptake and cytotoxicity in brain melanoma cells due to synergistic bioadhesive effects [165,166]. Methotrexate-loaded chitosan and glycol chitosan

nanoparticles demonstrated cytotoxic effects against C6 glioma cells and overcame multidrug resistance in MDCKII-MDR1 cell lines [167,168]. Furthermore, lipid–drug-conjugated nanoparticles carrying fluorouracil (5-FU) improved the efficacy of chemotherapy for glioma cells both in vitro and in vivo [169,170]. These advances highlight the critical role of nanoparticle-based systems in developing targeted and effective brain cancer therapies.

Breast cancer is one of the leading causes of cancer-related deaths worldwide, with tumors spreading through uncontrolled cell proliferation and invasion via the lymphatic system when malignant [171,172]. According to the World Health Organization (WHO), cancer accounts for approximately 13% of global deaths, resulting in around 8.2 million fatalities annually [173]. Among cancers affecting women, breast cancer is the most prevalent and causes higher mortality rates than even lung cancer [174]. In 2012, there were an estimated 1.7 million new cases of female breast cancer, accounting for 25% of cancer deaths globally [175]. The *Global Cancer Statistics 2020: GLOBOCAN* report, which analyzes cancer incidence and mortality across 36 cancer types in 185 countries, updated these figures, estimating 19.3 million new cancer cases (18.1 million excluding non-melanoma skin cancer) and nearly 10 million cancer-related deaths (9.9 million excluding non-melanoma skin cancer) in 2020 [176]. Notably, female breast cancer surpassed lung cancer as the most commonly diagnosed cancer, with around 2.3 million new cases (11.7%), followed by lung (11.4%), colorectal (10%), prostate (7.3%), and stomach (5.6%) cancers [177].

Treatment for breast cancer typically involves surgery, chemotherapy, radiation therapy, hormonal therapy, and targeted therapy [178]. Recently, nanotechnology has emerged as a promising approach in breast cancer treatment, with both organic and inorganic nanocarriers being utilized for targeted drug delivery [179]. Nanocarriers improve the solubility of hydrophobic anticancer drugs and ensure precise drug targeting [180]. Organic nanocarriers include polymeric nanoparticles, liposomes, and solid lipid nanoparticles, while inorganic types include magnetic nanoparticles, quantum dots, and carbon nanotubes (CNTs), all demonstrating significant potential in advancing breast cancer therapy [181].

Organic Nanomaterials in Breast Cancer Treatment

In the treatment of breast cancer, a number of organic nanomaterials have been investigated for targeted medication delivery. Letrozole (LTZ) and folic acid have been incorporated into solid lipid nanoparticles (SLNPs) that target folic acid receptors. These nanoparticles showed notable cell membrane damage when tested in vitro on MCF-7 breast cancer cell lines using MTT and lactate dehydrogenase (LDH) assays. TUNEL and Caspase-3 activity tests were used to confirm apoptosis induction [182,183]. The effectiveness of curcumin-loaded SLNPs (CURC-SLNPs) in combination with doxorubicin (DOX) against triple-negative breast cancer was investigated. According to in vitro findings, CURC-SLNPs successfully increased toxicity in cancer cells that expressed P-glycoprotein by five to ten times the cytotoxicity of curcumin in its free form [184,185].

Copolymer–magnetite nanoparticles composed of doxorubicin–core-shell chitosan conjugates were tested against HER2-overexpressing breast cancer cells. These anti-HER2-conjugated chitosan graft pluronic F127 nanoparticles proved effective as drug carriers for targeted anticancer therapy [186,187].

PEGylated ϵ -poly-l-lysine polymeric nanoparticles carrying both doxorubicin and lapatinib were evaluated on MCF-7 breast cancer cell models. This combination therapy delivered via DMMA-P-DOX/LAP nanoparticles significantly reduced or completely eliminated solid tumors in the tested models [188,189].

Inorganic Nanomaterials in Breast Cancer Treatment

Drug delivery for breast cancer has also made use of inorganic nanomaterials such magnetic nanoparticles and colloidal gold. Using gum acacia as a polysaccharide-based carrier, gemcitabine-hydrochloride (GEM) loaded onto colloidal gold nanoparticles was tested in vitro on the MDA-MB-231 breast cancer cell line. The chemotherapeutic medication was delivered to human breast cancer cells with precision thanks to these nanoparticles [190,191].

L-carnosine-coated magnetic nanoparticles (CCMNPs) were evaluated both in vitro and in vivo for their therapeutic effects. These nanoparticles showed high precision in targeting breast cancer cells, leading to a significant reduction in tumor mass without causing systemic toxicity [192,193].

Lung Cancer and Nanocarrier-Based Treatment

The lungs, essential for respiration, consist of airways that channel air in and out, and alveoli that serve as gas exchange sites [194,195]. While the airways form a robust barrier to particle entry, the alveolar wall and capillaries in the gas exchange region are comparatively fragile [196]. This extensive alveolar surface area and efficient blood-air exchange make the lungs more vulnerable to environmental damage, which can contribute to pulmonary diseases such as lung cancer [197]. To overcome the limitations of conventional therapies, various nanoparticles are being developed for respiratory applications. These nanocarriers facilitate treatment for lung disorders including asthma, tuberculosis, emphysema, cystic fibrosis, and cancer [198,199].

Recent advancements in nanoparticle-based lung cancer treatment include:

1. **Poly (L-aspartic acid co lactic acid)/DPPE copolymer nanoparticles** administered via intraperitoneal injection in mouse xenograft models. These nanoparticles, loaded with doxorubicin (DOX), have been applied to treat lung melanoma [200,201].
2. **Poly (β -amino ester) nanoparticles (PBAE)** delivered through intratumoral injection in mouse xenograft models. These self-assembling PBAE polymers complexed with DNA have been tested for transfection efficiency in p53 mutant H446 small cell lung cancer (SCLC) cells [202,203].
3. **Lipid-polymeric nanoparticles** administered intraperitoneally in mice, co-designed with epidermal growth factor (EGF) and loaded with cisplatin and doxorubicin to target lung carcinoma [204].
4. **Co-loaded doxorubicin and cisplatin nanoparticles** delivered via pulmonary administration in mouse models. Methoxy poly-(ethylenimine)-poly(l-glutamate) copolymers were developed to facilitate codelivery of DOX and CDDP for treating metastatic lung melanoma [205,206].
5. **Redox-responsive and pH-sensitive nanoparticles**, prepared through emulsification and solvent evaporation, loaded with Erlotinib (ETB) and modified with PAA-ss-OA. These were administered subcutaneously in mouse xenograft models targeting non-small cell lung cancer (NSCLC) [207].
6. **Nanoparticle-mesenchymal stem cell (MSC) systems**, where MSCs were loaded with nanoparticles carrying anticancer drugs and administered in rabbits, mice, and monkeys. MSCs demonstrated superior drug uptake compared to fibroblasts, effectively targeting lung melanoma [208,209].
7. **Hyaluronic-acid-based lipid nanoparticles** studied in vitro using dialysis techniques to enhance the efficacy of apigenin (APG) as an Nrf2 inhibitor in combination with docetaxel for NSCLC treatment [210].
8. **MAGE-A3 near-infrared (NIR) luminescent nanoparticles**, applied in vitro and in vivo (mouse models). These hybrid theranostic nanomaterials, coupled with Afatinib, were developed for in situ treatment of lung adenocarcinoma [211].
9. **Hyaluronic-acid-based nanoparticles** tested in vitro and in vivo for targeted delivery of paclitaxel to carcinoma cells. These nanoparticles were shown to overcome drug resistance and effectively inhibit cancer cell growth [212].

Drug Delivery Approaches in Heart Diseases

Cardiovascular diseases encompass a wide range of conditions, including myocardial infarction (MI) [213], ischemic injury, coronary artery disease (CAD), heart arrhythmias, pericardial disease, cardiomyopathy, and congenital heart defects [214,215]. These conditions are among the leading causes of death and disability worldwide [216]. Heart diseases often involve abnormalities in heart structure, impaired function, and damage to cardiac muscle tissue, along with ongoing remodeling and fibrosis [217,218]. Nearly half of MI patients die within five years, highlighting the urgent need for effective therapeutic strategies [216].

This demand has driven advancements in targeted drug delivery to the heart [219], aiming to prevent heart failure following MI [220]. Various nanocarriers have been explored for this purpose, including liposomes, silica nanoparticles, dendrimers, cerium oxide nanoparticles, micelles, titanium dioxide (TiO₂) nanoparticles, stents with nanocoatings, microbubbles, and polymer-drug conjugates. Among these, **magnetic nanoparticles** such as magnetoliposomes (MLs), which combine liposomes with magnetic nanoparticles, have emerged as promising tools for magnetically targeted drug delivery [221]. PEGylation of MLs prolongs their circulation time in blood, while conjugation with antibodies enhances active targeting to specific sites [222].

Namdari and colleagues demonstrated the potential of liposome-based carriers in a murine MI model. Modified nanocarriers — including cationic liposomes, perfluorocarbon nanoparticles, polyelectrolyte nanoparticles, and polymeric nanoparticles — have been engineered to improve drug loading and delivery efficiency into cells [223].

Examples of Nanocarrier Applications in Heart Disease

1. **Polymeric (PLGA) nanoparticles** tested in balloon-injured carotid and stented porcine coronary artery models in rats, loaded with AG-1295 and AGL-2043, showed significant inhibition of restenosis [224–230].
2. **Perfluorocarbon nanoparticles** applied in human plasma clots and hyperlipidemic animal models, carrying a3b integrins, surface-bound streptokinase, and other agents, demonstrated fibrinolytic activity in vitro and therapeutic potential in vivo [231–235].
3. **Cationic nanoparticles** examined in clinical trials involving patients with 60–99% arterial narrowing, delivered via catheter, showed notable improvement in myocardial perfusion. These nanoparticles delivered vascular endothelial growth factor (VEGF) through a viral vector [236–241].
4. **VEGF nanoparticles**, tested in murine models of myocardial infarction, successfully promoted angiogenesis and improved myocardial perfusion, aiding heart repair in coronary disease [242–245].

Drug Delivery Approaches in Skin Diseases

Follicular and cutaneous illnesses are two broad categories for skin diseases. Nanotechnology is becoming more and more important in modern treatments because it can deliver medications more efficiently and with fewer adverse effects.

Creams, gels, and ointments are examples of traditional formulations that frequently fall short of adequately penetrating skin tissues. Polymeric, lipid-based, and surfactant nanocarriers have been created to get around this restriction.

For instance, polymeric micelles enhance drug penetration into skin layers and are very useful in the treatment of skin malignancies. Research has demonstrated that by enhancing penetration into both the dermal and epidermal layers, chitosan polymeric nanoparticles, liposomes, and gold nanoparticles can improve drug delivery for disorders including atopic dermatitis [246].

Gold nanoparticles, owing to their extremely small size, penetrate the skin efficiently with minimal toxicity and no damage, making them a highly promising option in nanocarrier-based therapies for skin diseases.

Drug Delivery Approaches in Bone Diseases

Bone diseases arise from various pathological factors, including fractures, trauma, osteoporosis, arthritis, infections, and other conditions. Bone regeneration is a highly complex process, and advances in nanotechnology have enabled the fusion of nanomaterials with biomaterials to enhance bone repair. This combination has significantly improved bone implantation and regeneration through the development of advanced bone bioscaffolds [247].

Mechanism of Drug Delivery[248]

Drug Delivery Approaches in Blood Diseases

Blood disorders encompass a variety of conditions, including hematopoietic disorders, iron deficiency, leukemia, anemia, hemophilia, platelet disorders, and blood cancers. Conventional chemotherapeutic treatments often harm the immune system and carry a high risk of mortality. Bone marrow transplants, while effective for certain conditions, are costly and complex procedures. For instance, thalassemia is treated with the chelating agent deferoxamine to remove excess iron from the bloodstream. Recent research has shown that siRNA-coated nanocomposites possess inhibitory effects on tumor cells in vivo [248]. However, the application of nanomedicine in treating blood disorders remains an area of ongoing research and development.

Future Challenges of Nanomedicine

Nanomedicine holds tremendous promise for transforming clinical care, particularly in treating cancers and reducing mortality and morbidity. Nonetheless, several challenges remain. Integrating nanomedicine into clinical practice involves overcoming regulatory, insurance, and public health barriers. At present, the U.S. Food and Drug Administration (FDA) has not established specific regulations for products containing nanomaterials. Additionally, the absence of standardized protocols for nanomaterials and concerns over their safety have limited funding from agencies such as the Environmental Protection Agency (EPA) and the National Institute for Occupational Safety and Health (NIOSH) [249]. These challenges must be addressed for nanomedicine to achieve its full clinical potential.

Conclusions

As a subfield of nanotechnology, nanomedicine is quickly becoming recognised as a potent and adaptable method of treating a wide range of illnesses. Nanoparticle-based drug delivery systems are showing promise as therapeutic tools in a variety of medical specialities. For instance, researchers at the University of California are creating methods to use targeted nanovesicles to deliver cardiac stem cells directly to damaged heart tissue, improving cell retention and repair. These developments imply that integrating nanotechnology and stem cell therapy will result in important medical gains. Notwithstanding the potential, safety, toxicity, and standardisation remain concerns with nanomedicine, necessitating further study and regulation. However, because these systems have the potential to overcome the drawbacks of conventional medicine, the need for targeted drug delivery based on nanoparticles is rising rapidly.

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